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1 Ionisation effects on the permeation of pharmaceutical compounds through  
2 silicone membrane

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7

8 **Abstract**

9 Silicone membrane is frequently used as an *in vitro* skin mimic whereby experiments  
10 incorporate a range of buffered media which may vary in pH. As a consequence of such  
11 variability in pH there is a corresponding variability in the degree of ionisation which in turn,  
12 could influence permeation through the mainly hydrophobic-rich membrane structure. This  
13 study reports the effect of pH on the permeation of five model compounds (benzoic acid,  
14 benzotriazole, ibuprofen, ketoprofen and lidocaine). For the five compounds analysed, each  
15 at three distinct percentages of ionisation, it was found that the greater extent of permeation  
16 was always for the more 'neutral', i.e. more greatly unionised, species rather than the anionic  
17 or cationic species. These findings fit with the theory that the hydrophobic membrane  
18 encourages permeation of 'lipid-like' structures, i.e. the more unionised form of compounds.  
19 However, results obtained with an Inverse Gas Chromatography Surface Energy Analyser  
20 (iGC SEA) indicate the membrane surface to be an electron dense environment. In the  
21 knowledge that unionised forms of compounds permeate (rather than the charged species)  
22 this negatively charged surface was not anticipated, i.e. the basic membrane surface did not  
23 appear to affect permeation.

24

25

26 **Keywords:** silicone; PDMS; transdermal; permeation; ionisation; pKa

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## 30 Introduction

31 Understanding the permeation of compounds through human skin is a complex issue  
32 and can be difficult to predict using *in vitro* methods currently available such as human skin  
33 equivalents, mathematical models and synthetic membranes [1]. Although limited in  
34 predictive ability, their development and application are encouraged as there is a general  
35 trend to move away from animal-based studies within the EU. Analytical techniques using  
36 synthetic membranes are particularly popular and are mainly concerned with the application  
37 of materials such as polymeric membranes, including polydimethylsiloxane (PDMS), more  
38 commonly referred to as silicone membrane [2]. PDMS is a material that has many industrial  
39 uses (for example, microfluidic devices [3], pervaporation [4, 5], separation [6, 7]) and is  
40 known to adsorb solvents [8]. In pharmaceutical analysis PDMS is used to mimic the skin  
41 layer in a system designed to incorporate a donor solution and receiver solution, the latter  
42 from which samples are taken for analysis to determine quantitatively the rate and extent of  
43 permeation within a pre-selected period of time [9]. From such data it is possible to predict  
44 the fate of a compound following application on to the skin surface which is essential for  
45 toxicological profiling and formulation development. Experiments based on these *in vitro*  
46 predictive systems use equipment known as Franz cells and are routinely used for analysing  
47 cosmetic, household and pharmaceutical compounds [10, 11]. Membrane materials such as  
48 PDMS are favourable amongst researchers for several reasons including their reproducible  
49 composition and thickness, simplicity of use and cost effectiveness [12]. The hydrophobic  
50 nature of the membrane allows a barrier effect to occur, as is seen *in vivo* and as long as  
51 certain criteria are met, i.e. permeation is through passive diffusion, the compound  
52 permeating is metabolically inert and the formulation does not contain a skin-specific  
53 permeability enhancer [13], then useful data relating to permeation can be attained.

54 When analysing compounds using skin (or skin mimics, such as PDMS) there is a  
55 vast array of donor phase compositions available. These range from simple water-based  
56 solutions of the compound under investigation [14] to compositions that replicate the  
57 complex formulations intended for market [15, 16]. For example, even when considering a  
58 model compound such as ibuprofen, previous studies have focussed on a basic aqueous  
59 solvent at a pre-selected pH through to the application of far more complex formulations,  
60 such as small amounts of ibuprofen gel, as would be applied to human skin [17] or the  
61 addition of surfactants [13]. It would appear that little attention has been paid to how, or why,  
62 particular solvents have been selected in the majority of cases for the donor phase although  
63 recent work within our group has begun to consider the importance of the presence of binary  
64 mixtures in the donor phase and effects of variation in the receptor phase [18]. From such  
65 work it is clear that the composition of the donor phase can, and does, influence permeation  
66 yet the extent to which this occurs is as yet unclear.

67 One particular aspect of all aqueous based formulations that can fundamentally dictate  
68 the physicochemical behaviour of the compound under investigation is the pH of the chosen  
69 solution. Through knowledge of the pKa of a compound it is possible to calculate the  
70 percentage ionised (with application of the Henderson-Hasselbalch equation (Eqtn. 1)) at any  
71 given pH where the unionised species (HA) is in equilibrium with the ionised species (A<sup>-</sup>).

$$72 \quad (1) \text{ pH} = \text{pKa} - \log ([\text{HA}]/[\text{A}^-])$$

73 Thus, it is possible to manipulate the pH of a solution so that the ratio of the concentration  
74 unionised ([HA]) to ionised ( $[A^-]$ ) can be controlled and known for any compound with a pre-  
75 determined pKa. Other physicochemical factors may also play a role in permeation, such as  
76 the octanol-water partition coefficient (logP) so for the compounds considered in this work a  
77 wide range of lipophilicities were considered to confirm the potential importance of this  
78 additional factor on permeation.

79 The ability of Franz cell-based experiments to predict the behaviour of a compound  
80 within a formulation has led some researchers to select donor phases with pH values similar  
81 to those found *in vivo*. For example, some studies have used an aqueous phase at a low pH to  
82 replicate the typical pH of skin or acne-prone skin [19] yet others have **selected pH values**  
83 **such as 7.4** [20]. Despite such studies implying an appreciation of how important it can be to  
84 select and control the pH of the donor phase, little research has been conducted prior to this  
85 study to investigate the role the relationship between pH and percentage ionisation can have  
86 on the subsequent extent of permeation in Franz cell studies. One particular study has  
87 investigated ionisation and the effect of absorption enhancers on the transport of one  
88 compound, namely salicylic acid, through silastic rubber and human skin [21]. In this study it  
89 was found that permeant concentration was directly related to the degree of ionisation of the  
90 solute, i.e. permeation conformed to the pH-partition hypothesis. **However**, only this one  
91 specific compound was considered in the work. Whether a similar relationship would be  
92 observed for a range of compounds was not considered, particularly with a range of drugs  
93 that ionise to form cationic and anionic species such as those studied in this work.

94

## 95 **Materials and Methods**

### 96 **Materials**

97 Polydimethylsiloxane membrane (PDMS) was used as purchased (ATOS Medical,  
98 Sweden) with a standard thickness of 130  $\mu\text{m}$  and cut to size as required.

99

100 The glassware used was of class B. Deionised water was used throughout the  
101 experiments. The flow-through diffusion cells were purchased from PermeGear Inc., USA.

102

### 103 **Methods**

#### 104 **Flow through permeation methodology**

105 In all experiments the concentration of the model compounds in the donor solution  
106 was 1 mg/mL **with a total volume of 0.8 mL per solution**. PDMS membrane was employed as  
107 a permeability barrier. The membrane was soaked in buffer solution for 30 minutes prior to  
108 being mounted in the flow-through diffusion cells. After assembly the integrity of each cell  
109 was checked visually by inversion. Phosphate buffer solution was pumped through the  
110 diffusion cells at a rate of 2 mL/h and collected by means of a fraction collector at the  
111 predetermined time interval. Extracted samples were analysed by means of UV spectroscopy  
112 to quantify the model compounds over a period of 7 hours (benzoic acid at 226 nm,  
113 benzotriazole at 262 nm, ibuprofen at 230 nm, ketoprofen at 264 nm and lidocaine at 219

114 nm). All experiments were conducted in triplicate with the mean value shown with standard  
115 deviation based error limits. All flow-through cells used in this study had a diffusion area of  
116  $0.554 \text{ cm}^2$ .

117

### 118 **iGC methodology:**

119 70 mg of PDMS membrane were packed into an iGC silanised glass column. The  
120 dispersive surface energy ( $\gamma_s^D$ ) and the acid-base free energy ( $\gamma_s^{AB}$ ) of adsorption were  
121 determined by running the sample at a series of surface coverage with alkanes and polar  
122 probe molecules. The sample column was pre-conditioned for 2 hours at 25 °C and 0 % RH  
123 with 10 mL/min helium carrier gas. The experiment was conducted at 25 °C with 10 mL/min  
124 total flow rate of helium, and using methane for dead volume correction.

125

## 126 **Results and Discussion**

### 127 **Permeation dependence with ionisation**

128 Five compounds were analysed to determine the amount permeated through silicone  
129 membrane, each at three specific percentages of ionisation (calculated using Equation 1) and  
130 pKa values of benzoic acid 4.2 [22], benzotriazole 8.2 [23], ibuprofen 4.9 [24], ketoprofen  
131 4.0 [25] and lidocaine 7.8 [26]. These compounds were selected for their diverse range of  
132 both pKa values and lipophilicities, the latter ranging from a logP of 1.2 for benzotriazole  
133 [27] to 3.6 for ibuprofen [28].

134 Previous work [21] investigated salicylic acid permeation to determine if it conformed  
135 to the pH-hypothesis whereby observed permeability coefficients and steady-state flux  
136 increased with decreasing pH and a linear relationship was found between the fraction  
137 unionised and flux. The results suggested that the change in flux was a direct consequence of  
138 pH, which controlled the concentration of undissociated species. However, their study only  
139 investigated one specific compound, namely salicylic acid. This study had the aim of  
140 determining if a similar relationship would be observed for a range of compounds with  
141 differing pKa and logP values, i.e. to identify if the flux-pH relationship can be applied more  
142 generally. Figures 1-5 display the cumulative amount permeated for all five compounds as a  
143 function of percentage unionised. Although it was not possible for all five compounds to  
144 achieve the same degrees of ionisation with their individual pKa values and the pH range  
145 available, the distribution of percentages allows a comparative study to be undertaken. It can  
146 be seen that in all cases there was a reduction in permeation as the percentage unionised  
147 decreased which would be expected based on the hydrophobic nature of the membrane.  
148 Through modifying the pH of the aqueous solution (for example from pH 8.5 for ketoprofen  
149 through to pH 4.5 for benzoic acid) it was interesting to observe a significant change in the  
150 degree of permeation over the experimental period of seven hours.

151 Considering the data in Figures 1-5, more specifically the relationship between the  
152 amount permeated after 7 hours and the percentage of compound unionised for each, then it  
153 can be concluded they all display a generally linear relationship with increasing amount  
154 permeated with increasing percentage unionised. A plot of such data allows comparisons to  
155 be made between the gradients, i.e. how influential the percentage ionised is on permeation

156 (data not shown). The most dramatic change in amount permeated as a function of percentage  
157 unionised was observed for ibuprofen and the least change was seen for benzotriazole,  
158 possibly as a consequence of the pKa with a value of 8.2 for benzotriazole [23].  
159 Alternatively, this may have been a consequence of the comparative logP values with  
160 ibuprofen displaying the greatest change in amount permeated and being the most  
161 hydrophobic of the compounds through to the least change observed for benzotriazole with  
162 this compound being the least hydrophobic. Benzoic acid did not show such a clearly linear  
163 relationship between the percentage unionised and amount permeated although the overall  
164 trend fitted with the data from the remaining compounds.

165 Flux values ( $\mu\text{g cm}^{-2} \text{h}^{-1}$ ) were calculated for each compound and plotted against the  
166 fraction unionised to determine if a linear relationship was apparent for all compounds or, if  
167 permeation was a more complex process and was dependent upon other factors, such as logP.  
168 This analysis was conducted in a similar manner to that of Smith and Irwin [21] whereby  
169 they observed a linear relationship for the one compound analysed, namely salicylic acid.  
170 Data for all five compounds can be found in Table 1.

171 As expected, a similar trend in the data was observed for that discussed above, i.e.  
172 from comparative consideration of the amount permeated with percentage unionised, as all  
173 experiments throughout the study were conducted for seven hours. Again, the relationship  
174 between flux and fraction unionised was mainly linear with the one exception of benzoic acid  
175 where the intermediate fraction of unionised solution appeared to allow more compound to  
176 permeate than expected. This anomaly was unexpected although the general trend was similar  
177 to that of the remaining compounds, i.e. flux increased as the percentage of unionised  
178 compound increased. One factor that can certainly be removed from consideration is the  
179 membrane thickness as this was consistent throughout the experimental study, the importance  
180 of maintaining membrane thickness has been reported previously by others [29].

181

## 182 **iGC membrane surface analysis**

183 The BET Specific Surface Area (BET-SSA) of the membrane was measured with the  
184 physical adsorption of ethanol by DVS (Table 2).

185

186

187 Dispersive ( $\gamma_s^D$ ), acid-base ( $\gamma_s^{AB}$ ) and total surface energy ( $\gamma_s^T$ ) profiles are shown in  
188 Figure 6 and indicate the sample is energetically heterogeneous, i.e. surface energy changed  
189 as a function of surface coverage with a major dispersive component contribution.

190

191

192 Heterogeneity was confirmed from the wide variation of surface active sites through  
193 plotting surface energy distributions (data not shown). Furthermore, the specific acid-base  
194 Gibbs free energy of adsorption ( $\Delta G_{SP}$ ) varied with surface coverage, confirming the  
195 heterogeneous nature of the sample. From analysing interactions with five polar probe  
196 molecules the rank order of decreasing  $\Delta G_{SP}$  was found to be

197 acetonitrile>ethanol>dichloromethane>acetone>ethyl acetate although the sample showed  
198 only a relatively small degree of interaction with all probes. Gutmann acid ( $K_a$ ) and base ( $K_b$ )  
199 values were calculated using  $\Delta G_{SP}$  values with  $K_b$  values consistently higher than  $K_a$ . These  
200 results confirm that the surface of the sample to be basic in nature and present a high  
201 concentration of electron-donating surface functional groups. It can be assumed these are un-  
202 substituted hydroxyl groups based on the chemistry of the material. These findings can be  
203 linked with the previously discussed permeation data to understand why it was always the  
204 more unionised form of a compound that favoured permeation. This can be explained in  
205 terms of the iGC data which indicates the surface is basic which one might expect would  
206 repel the ionised form of basic compounds (such as lidocaine) and weakly bond the ionised  
207 form of the acid compounds (benzoic acid, benzotriazole, ibuprofen and ketoprofen). In  
208 either case, the ionised form is less inclined to permeate the negatively charged membrane  
209 surface compared with the unionised form.

210

## 211 Conclusion

212 From considering permeation results in conjunction with iGC data it can be seen that  
213 data presented based on permeation indicates there is a general preference for permeation for  
214 the most unionised species for all compounds. Based on these findings it can be concluded  
215 that the general hydrophobic nature of the membrane outweighs the effects of any surface  
216 groups that may be present. Alternatively, it may be the case that the existence of a peripheral  
217 layer of basic groups creates an electrostatic attraction or repulsion for the ionised forms of  
218 drugs, preventing permeation from occurring. In either case, it is clear that permeation is  
219 more favourable for the more unionised form of a compound despite the presence of a basic  
220 PDMS surface.

221

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225

## 226 References

227

- 228 [1] L.J. Waters, Recent developments in skin mimic systems to predict transdermal permeation.,  
229 *Current Pharmaceutical Design* 21 (2015) 2725 - 2732.  
230 [2] S. Oshima, C. Suzuki, R. Yajima, Y. Egawa, O. Hosoya, K. Juni, T. Seki, The use of an artificial skin  
231 model to study transdermal absorption of drugs in inflamed skin, *Biological and Pharmaceutical*  
232 *Bulletin*, 35 (2012) 203-209.  
233 [3] J.N. Lee, C. Park, G.M. Whitesides, Solvent Compatibility of Poly(dimethylsiloxane)-Based  
234 Microfluidic Devices, *Analytical Chemistry*, 75 (2003) 6544-6554.  
235 [4] S. Koter, A. Kujawska, W. Kujawski, Modeling of transport and separation in a  
236 thermopervaporation process, *Journal of Membrane Science*, 480 (2015) 129-138.

237 [5] Z. Dong, G. Liu, S. Liu, Z. Liu, W. Jin, High performance ceramic hollow fiber supported PDMS  
238 composite pervaporation membrane for bio-butanol recovery, *Journal of Membrane Science*, 450  
239 (2014) 38-47.

240 [6] P. Li, H.Z. Chen, T.S. Chung, The effects of substrate characteristics and pre-wetting agents on  
241 PAN-PDMS composite hollow fiber membranes for CO<sub>2</sub>/N<sub>2</sub> and O<sub>2</sub>/N<sub>2</sub> separation, *Journal of*  
242 *Membrane Science*, 434 (2013) 18-25.

243 [7] S.A. Stern, Polymers for gas separations: The next decade, *Journal of Membrane Science*, 94  
244 (1994) 1-65.

245 [8] P.M. Van Midwoud, A. Janse, M.T. Merema, G.M.M. Groothuis, E. Verpoorte, Comparison of  
246 biocompatibility and adsorption properties of different plastics for advanced microfluidic cell and  
247 tissue culture models, *Analytical Chemistry*, 84 (2012) 3938-3944.

248 [9] K.B. Sloan, J. Synovec, H. Ketha, A surrogate for topical delivery in human skin: Silicone  
249 membranes, *Therapeutic Delivery*, 4 (2013) 203-224.

250 [10] L. Bartosova, J. Bajgar, Transdermal drug delivery in vitro using diffusion cells, *Current*  
251 *medicinal chemistry*, 19 (2012) 4671-4677.

252 [11] B. Baert, J. Boonen, C. Burvenich, N. Roche, F. Stillaert, P. Blondeel, J. van Boclaer, B. de  
253 Spiegeleer, A new discriminative criterion for the development of franz diffusion tests for  
254 transdermal pharmaceuticals, *Journal of Pharmacy and Pharmaceutical Sciences*, 13 (2010) 218-  
255 230.

256 [12] S.F. Ng, J.J. Rouse, F.D. Sanderson, G.M. Eccleston, The relevance of polymeric synthetic  
257 membranes in topical formulation assessment and drug diffusion study, *Archives of Pharmacol*  
258 *Research*, 35 (2012) 579-593.

259 [13] L. Waters, L. Dennis, A. Bibi, J.C. Mitchell, Surfactant and temperature effects on paraben  
260 transport through silicone membranes, *Colloids and Surfaces B: Biointerfaces*, 108 (2013) 23-28.

261 [14] S. Majumdar, J. Thomas, S. Wasdo, K.B. Sloan, The effect of water solubility of solutes on their  
262 flux through human skin in vitro, *International Journal of Pharmaceutics*, 329 (2007) 25-36.

263 [15] R.M. Watkinson, R.H. Guy, G. Oliveira, J. Hadgraft, M.E. Lane, Optimisation of cosolvent  
264 concentration for topical drug delivery III - Influence of lipophilic vehicles on ibuprofen  
265 permeation, *Skin Pharmacology and Physiology*, 24 (2010) 22-26.

266 [16] R.M. Watkinson, C. Herkenne, R.H. Guy, J. Hadgraft, G. Oliveira, M.E. Lane, Influence of  
267 ethanol on the solubility, ionization and permeation characteristics of ibuprofen in silicone and  
268 human skin, *Skin Pharmacology and Physiology*, 22 (2009) 15-21.

269 [17] C. Herkenne, A. Naik, Y.N. Kalia, J. Hadgraft, R.H. Guy, Ibuprofen transport into and through  
270 skin from topical formulations: In vitro-in vivo comparison, *Journal of Investigative Dermatology*,  
271 127 (2007) 135-142.

272 [18] Y. Shahzad, L.J. Waters, C. Barber, Solvent selection effects on the transport of compounds  
273 through silicone membrane, *Colloids and Surfaces A: Physicochemical and Engineering Aspects*,  
274 458 (2014) 96-100.

275 [19] C. Guo, R.H. Khengar, M. Sun, Z. Wang, A. Fan, Y. Zhao, Acid-Responsive Polymeric  
276 Nanocarriers for Topical Adapalene Delivery, *Pharmaceutical Research*, (2014).

277 [20] P.S. Mertz, K.B. Sloan, The flux of select NSAIDs through silicone membranes from mineral oil,  
278 *Pharmaceutics*, 6 (2014) 354-365.

279 [21] J.C. Smith, W.J. Irwin, Ionisation and the effect of absorption enhancers on transport of  
280 salicylic acid through silastic rubber and human skin, *International Journal of Pharmaceutics*, 210  
281 (2000) 69-82.

282 [22] Z. Wang, H. Deng, X. Li, P. Ji, J.P. Cheng, Standard and absolute pKa scales of substituted  
283 benzoic acids in room temperature ionic liquids, *Journal of Organic Chemistry*, 78 (2013) 12487-  
284 12493.

285 [23] F.J. Benitez, J.L. Acero, F.J. Real, G. Roldán, E. Rodríguez, Ozonation of benzotriazole and  
286 methylindole: Kinetic modeling, identification of intermediates and reaction mechanisms, *Journal*  
287 *of Hazardous Materials*, 282 (2015) 224-232.

- 288 [24] S.C. Paul, L.J.M. Githinji, R.O. Ankumah, K.R. Willian, G. Pritchett, Sorption behavior of  
289 ibuprofen and naproxen in simulated domestic wastewater, *Water, Air, and Soil Pollution*, 225  
290 (2014).
- 291 [25] M. Fillet, I. Bechet, V. Piette, J. Crommen, Separation of nonsteroidal anti-inflammatory drugs  
292 by capillary electrophoresis using nonaqueous electrolytes, *Electrophoresis*, 20 (1999) 1907-1915.
- 293 [26] H. Liu, J. Atkins, R.S. Kass, Common molecular determinants of flecainide and lidocaine block  
294 of heart Na<sup>+</sup> channels: Evidence from experiments with neutral and quaternary flecainide  
295 analogues, *Journal of General Physiology*, 121 (2003) 199-214.
- 296 [27] D.S. Hart, L.C. Davis, L.E. Erickson, T.M. Callender, Sorption and partitioning parameters of  
297 benzotriazole compounds, *Microchemical Journal*, 77 (2004) 9-17.
- 298 [28] L.J. Waters, S. Bedford, G.M.B. Parkes, J.C. Mitchell, Influence of lipophilicity on drug-  
299 cyclodextrin interactions: A calorimetric study, *Thermochimica Acta*, 511 (2010) 102-106.
- 300 [29] G. Firpo, E. Angeli, L. Repetto, U. Valbusa, Permeability thickness dependence of  
301 polydimethylsiloxane (PDMS) membranes, *Journal of Membrane Science*, 481 (2015) 1-8.

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